



Cardiovascular: PLATELET - THROMBOSIS - ADHESION ASSAY

INTRODUCTION

Cellix Ltd. have developed a novel microflow system consisting of a novel syringe pump with microfluidic biochip and flow sensor controlled by a PC using dedicated software. The microfluidic syringe pump allows very accurate flow rates to be achieved that are more reproducible and consistent than anything currently available. Importantly, flow rates are very low (5 pL min^{-1} to $10 \text{ }\mu\text{L min}^{-1}$) and the shear stress levels that the pump can mimic (up to 30 dyne cm^{-2}) are equivalent to those found in blood vessels *in vivo*. The biochips are comprised of eight different channels, and can be manufactured so that the dimensions of the channel are similar to the blood vessel being assessed. Currently, the channels are able to be coated with recombinant human adhesion proteins for use in inflammation studies. However, it should soon be possible to culture a desired cell line on the channel surface, allowing for more physiologically relevant assays to be completed. The microfluidic syringe pump is vital to the use of small diameter channels as standard syringe pumps are incapable of delivering the required low flow rates.

OVERVIEW

First of all, the cell type to be analysed must be determined, followed by establishing how to harvest such cells e.g. culturing in growth media, or isolation from *in vivo* fluids. Secondly, the assay itself should be outlined, including whether live cells or proteins will be coating the channels of the biochip. If it is the former, protocols for culturing the cells both outside and inside the biochip channel must be established. Thirdly, the adhesion profile of the cells to be passed through the coated channel should be determined. Next, if exogenous compounds are being analysed, these should then be introduced to the system and their effect on the adhesion profile assessed. This should include calculation of required concentrations and pre-incubation conditions, before introduction to the system. Finally, the images taken via the digital camera attached to the microscope should be masked and analysed using the Duocell software.

ASSAY DEVELOPMENT STEPS

i) Choice of cell type and harvesting protocols

A microfluidic assay assessing the adhesion profile of platelets on various matrix proteins was developed. Blood was collected

from healthy volunteers who were not taking any medication and were free from aspirin and other anti-platelet agents within the preceding 2 weeks. The blood was drawn by venepuncture into tubes containing a 1:10 volume of 3.8% (wt/vol) trisodium citrate, which is a calcium chelator, and gently mixed. The anti-coagulant agent D-phenylalanyl L-propyl-L-arginine chloromethyl ketone dihydrochloride (PPACK), which is a thrombin inhibitor, was added to a final concentration of $80 \mu\text{M}$ in whole blood. The first 5ml of drawn blood was discarded. Whole blood can be kept in 50ml polypropylene tubes during assay procedures. Platelets in whole blood were labelled by incubating anti-coagulated blood with the fluorescent dye DiOC6 ($1 \mu\text{M}$) for 10-20mins, (Blood Platelet count varied from $136\text{-}273 \times 10^3 \text{ platelets } \mu\text{l}^{-1}$).

ii) Assay outline, including chip coating procedures

Each microchannel was coated overnight in humid conditions at 4°C with either vWF (von Willebrand Factor, $100 \mu\text{g/ml}$) or collagen (HORM Equine Fibrillar Collagen, $200 \mu\text{g/ml}$). All channels were then coated with BSA (Bovine Serum Albumin, $10 \mu\text{g/ml}$) to occupy non-specific binding sites. An additional channel was coated with BSA ($10 \mu\text{g/ml}$) for 2hrs at room temperature. Prior to shear experiments, all channels were washed thrice with PBS.

iii) Adhesion profiles

Whole blood was infused into the vWF, collagen and BSA coated channels under a defined shear stress, ranging from 0 to 120 dyne cm^{-2} , two minute per shear stress level. Images at the indicated shear stress level were captured using the accompanying MetaMorph imaging software (1 frame per second). Adhesion of platelets and thrombus formation was evaluated by monitoring platelet migratory behaviour in real time with images captured via a Liquid chilled Quantix 10-57 CCD camera connected to the Zeiss Axiovert 200 Inverted Epi-Fluorescence microscope.

iv) Image analysis

Images for analysis have been extracted from video at frames 1, 30, 60 and 120. The thrombus profile was recorded using Duocell application software. Data was exported into Excel for interpretation. Data was presented as $\text{mean} \pm \text{s.e. mean}$.



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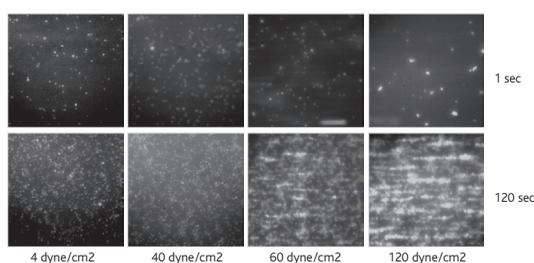


Figure 1: Platelet adhesion profile on vWF at indicated time points (1 and 120sec), subjected to gradient shear stress of (4, 40, 60 and 120 dyne/cm²).

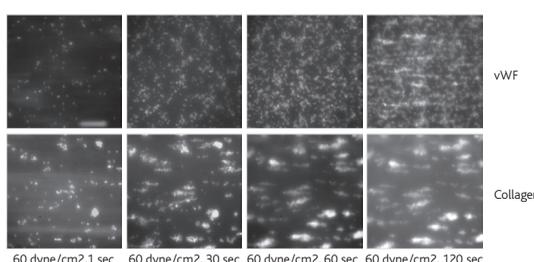


Figure 3: Platelet adhesion profile to vWF and collagen at constant shear stress of 60 dyne/cm², at indicated time points.

RESULTS

The adhesion profile of platelets was recorded with respect to vWF, collagen and BSA (data not shown). Whole blood infused into vWF-coated channels at a range of shear stresses show rolling/adhesion of platelets after just 1sec. At 120sec, lower shear stress (4 and 40 dyne cm⁻²) result in platelets rolling/adhesion, whereas, at higher stress (60 and 120 dyne cm⁻²) platelet thrombus formation appears (Figure 1). A threshold limit of approximately 60 dyne cm⁻² is required for thrombus formation, conditions that occur in microcirculation. Chain-like structures of platelets aligned in the direction of flow (120sec at higher shear stress) result in the number of individual platelets interacting with immobilised vWF to be reduced. Using Duocell software to analyse the thrombus formation profile at 120sec, the average length of the aggregates (thrombus) was calculated. A 5.9 fold increase in thrombus formation from 4 dyne cm⁻² to 120 dyne cm⁻² was recorded (Figure 2(i)). The varying length (maximum, minimum and average) of the distributed aggregates is represented in Figure 2(ii).

Collagen is a unique agonist of platelets, acting as an immobilised legend that only causes platelet activation after stable adhesion. Activated platelet thrombus formation is evident as early as 1sec when whole blood is infused into the collagen-coated channel at a shear stress of 60 dyne cm⁻², intensifying over the course of 120sec (Figure 3). Distinct thrombus formation is noted on collagen - in contrast to vWF-coated channels.

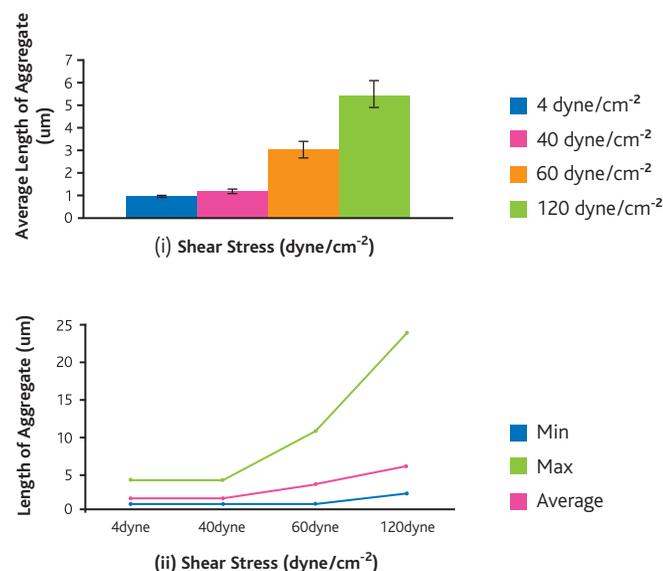


Figure 2: Platelet adhesion to vWF showing (i) the average length of the aggregates (thrombus) at various shear stresses and (ii) the minimum, maximum and average length of the aggregates at the various shear stresses.

ASSAY CONDITIONS

The following solutions were used during the above procedure:

JNL Buffer (wash buffer for inlets/outlets tubing)

JNL Buffer (100mls) = JNL A (10ml), JNL B (10ml), JNL D (10ml) and JNL E (1ml)

[JNL A: 60mM Dextrose, JNL B: 1.3M NaCl, 90mM Na Bicarb, 100mM Na Citrate (Tribasic, dehydrate), 100mM Tris base, 30mM KCl, JNL D: 8.1mM KH₂PO₄ (monobasic anhydrate), JNL E: 90mM MgCl₂·6H₂O]

Adjust pH 7.35 with 49ml Acid Citrate Dextrose (Citrate acid anhydrous 38mM, Sodium citrate 75mM, Dextrose 136mM) Incubate at room temperature for 5mins. Add 20ml H₂O, incubate at RT.

ACKNOWLEDGEMENTS

We thank Dr. Gerardene Meade and Prof. Dermot Kenny, Molecular and Cellular Therapeutics, Royal College of Surgeons in Ireland for carrying out the platelet adhesion studies.

REFERENCES

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